

Available online at : http://jitce.fti.unand.ac.id/

JITCE (Journal of Information Technology and Computer Engineering)

| ISSN (Online) 2599-1663 |



Intelligent 3D Analysis for Detection and Classification of Breast Cancer

Suzani Mohamad Samuri, Try Viananda Nova Megariani

Computing Department, Faculty of Art, Computing and Creative Industry, Universiti Pendidikan Sultan Idris

ARTICLE INFORMATION

Received: June 13th, 2019 Revised: November 8th, 2019 Available online: November 11th, 2019

KEYWORDS

3D analysis, fuzzy logic, contrast enhancement, feature selection, computer aided diagnosis (CAD)

CORRESPONDENCE

E-mail: suzani@fskik.upsi.edu.my

ABSTRACT

Breast cancer continues to be a significant public health problem in the world. Early detection is the key for improving breast cancer prognosis. Mammography has been one of the most reliable methods for early detection of breast carcinomas. However, it is difficult for radiologists to provide both accurate and uniform evaluation for the enormous mammograms generated in widespread screening. Breast cancer computer aided diagnosis (CAD) systems can provide such help and they are important and necessary for breast cancer control. Micro calcifications and masses are the two most important indicators of malignancy, and their automated detection is very valuable for early breast cancer diagnosis. Since masses are often indistinguishable from the surrounding parenchymal, automated mass detection and classification is even more challenging. This research presents algorithms for building a classification system or CAD, especially to obtain the different characteristics of mass and micro calcification using association technique based on classification. Starting with an individual-specific deformable of 3D breast model, this modelling framework will be useful for tracking visible tumors between mammogram images, as well as for registering breast images taken from different imaging modalities. From the results, the classifier developed able to perform well by successfully classifying the cancer and non-cancer (normal) images with the accuracy of 97%. Apart from that, by applying color map to the final results of segmentation provides a more interesting display of information and gives more direction to the purpose of image processing, which distinguishes between cancerous and non-cancerous tissues.

INTRODUCTION

Breast cancer is the leading cause of death for women, accounting for 14% of cancer mortalities in 2008 [1]. Early detection through X-ray mammography screening has been shown to reduce the mortality rate of this disease [2]. However, X-ray mammography imaging has its limitations, being unable to detect and distinguish with 100% accuracy the abnormalities in the breast [3]. Other imaging modalities, such as ultrasound and magnetic resonance imaging (MRI), are therefore used in conjunction with X-ray mammography to image the breasts [4]. Most of the breast cancer is detected by the presence of micro calcification [5]. Mammogram readings are usually performed by a radiologist. Variety of factors such as the poor quality of the image, eye fatigue factor, the performance of radiologist could greatly affect the diagnose results [6]. To overcome this problem, several computer aided diagnosis systems (CAD) are developed by researchers in this field for automatic detection of breast cancer [7-10]. This research presents a method for building a classification system or CAD based on 3D analysis, especially to obtain the different characteristics of mass and micro calcification [11-13] using association technique based on classification. The classification process mainly consists of two phases: training phase and testing phase. In the training phase the properties of typical image features are isolated and the training samples are having their object class information. In this study, the statistics features and the Gray Level Co-occurrence Matrix (GLCM) [14-17] based on texture features are extracted. Feature selection is an important step before the process of any classification scheme. In terms of the data used, the importance of data cleaning is considered. The data cleaning is applied in the context of image content mining. 3D analysis of the breast images [19] was used to develop a computational intelligence algorithm for tracking visible cancerous cells between images, as well as for registering breast images taken from different imaging modalities.

This study finds the different characteristics of micro calcification and mass [20-22]. The information of centroid and radius provided in Mammographic Image Analysis Society (MIAS) database [23] are used to find and extract the micro calcification and mass. The finding is the candidate regions in mammogram into two categories: micro calcification and mass regions. This finding will help radiologists in their tasks to detect subtle abnormalities in a mammogram. Furthermore, it also helps in making a decision whether a biopsy procedure is necessary or not. A decision of the candidate regions were carefully concluded, especially in selecting the threshold value and size of the candidate regions in order to obtain the candidate regions that highly resemble micro calcification or mass [24-26]. Unfortunately, there are large variations of threshold value from one image to the others, therefore a constant threshold will not be good enough.

The paper is organized as follows; Section I is an introduction and background. Section II provides the detail proposed methodology for micro calcification and mass detection. Section III discusses the experiment results. Finally, Section IV presents the concluding remarks.

METHOD

In this section, the CAD detection scheme involving stage mass is described in Figure 1. Starting with pre-processing image of digital mammograms to reduce noise and improve the contrast of images [27-30], then, the segmentation of the image defined by the majority of articles about the detection of a mass as the location of the suspicious mass. In the third stage, features taken and was chosen to classify the type of lesion or remove false positive. Then, detection and classification of a mass were done. All these work were done using MATLAB 2018b software.

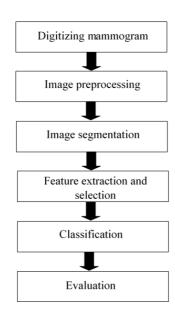


Figure 1. The CAD detection scheme

RESULTS AND DISCUSSION

Digitizing Mammogram

At this stage, 100 mammograms data were collected from the Central Pertamina Hospital, Indonesia (50 normal data and 50 cancer) as shown in Figure 2.

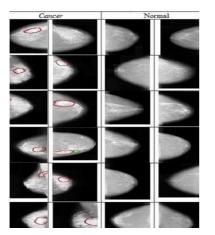


Figure 2. Some of the mammogram of normal and cancer images.

Image Pre-processing

Several stages involved in image pre-processing to improve image quality as shown in Figure 3, and the results from this preprocessing is shown in Figure 4, where the 3D cancer and normal images can be analyzed and fed to the next process which is the image segmentation.

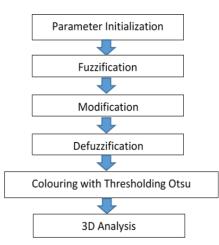


Figure 3. The flowchart of pre-processing stages

In this case, fuzzification involves transforming a crisp quantity into a fuzzy quantity. This can be achieved by identifying the various known crisp and deterministic quantities as completely nondeterministic and quite uncertain in nature. While defuzzification involves converting the fuzzy results into crisp results. This process is capable of generating a non-fuzzy control action which illustrates the possibility distribution of an inferred fuzzy control action. After the process of defuzzification, the thresholding Otsu is used to perform automatic image thresholding [31] by minimizing intra-class intensity variance, or equivalently, by maximizing inter-class variance [32]. The algorithm has been improved to include color scheme to better shown the segments of the breast cancer.

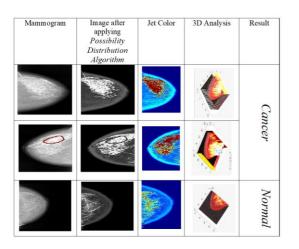
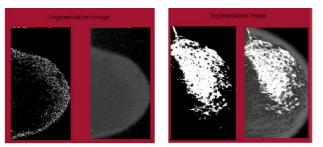


Figure 4. Results from the pre-processing of cancer and normal images

Image Segmentation

At this stage, Thresholding Otsu algorithm [33-35] is used to segment the pictures by means of distinguished it to the 2 classes , namely background (value set to 0 and object (value set to 1) use as a certain level of a parapet. As the result from this segmentation, it can be clearly seen that there are very significant differences between normal and cancer images, in such a way that a mass of data on cancer more than the normal. Figure 5 shows segmentation results from normal image and cancer image.



(a) Segmentation of normal image

(b) Segmentation of cancer image

Figure 5. Segmentation results from normal and cancer images

Feature Extraction and Selection

For feature extraction, GLCM (Grey Level Co-occurrence Matrix) is being used. GLCM is the two dimensions represent the level variation gray at the image. GLCM is one of the popular statistical methods of extracting textural feature from images. According to [36], by extracting the features of an image by GLCM approach, the image compression time can be greatly reduced in the process of converting RGB to Gray level image when compared to other discrete wavelet transform (DWT) techniques. In this study, measurement of the correlation, energy, in contrast, entropy, and homogeneity are computed as features extracted and shall be used in the classification stage. Table 1 shows some of the results from GLCM.

Classification

Neural network is a model that made to imitate the function of learning that owned the human brain .In the neural network, layer neurons were brought in, called neurons layer .Usually each neuron connected to all of a layer of neurons are in the back and front of him except layer input and output. Information sent in a neural network propagation layer started from the input to output through one or more hidden layers. Multilayer Perceptron (MLP) neural network is used in this study to classify the image to be cancer or normal.

Evaluation

For evaluation, this study used 60 samples, in which 30 of the samples are of cancer images and 30 of them are normal images. As the results from this evaluation, it is found out that only 2 cancer images that could not be classified. This may be due to fat or the images contain spicules. Therefore, the overall performance of the classifier developed is very good with the accuracy of 97%. Table 2 shows some of the example from the evaluation stage.

Table 1. Some of the results from GLCM

Images	Contrast	Variance	Std Dev	Kurtosis	Mean	Smoothness
1	1.027975	0.395393	0.628802	9.451290	0.539653	0.283356
2	1.441665	0.479333	0.692339	9.469165	0.592580	0.324020
3	0.745201	0.368605	0.607128	7.047246	0.533764	0.269329

Table 2. Some of the evaluation results

Images	Contrast	Variance	Std Dev	Kurtosis	Mean	Smoothness	Correct	Incorrect
1	1.027975	0.395393	0.628802	9.451290	0.539653	0.283356	50%	50%
2	1.441665	0.479333	0.692339	9.469165	0.592580	0.324020	50%	50%
3	0.745201	0.368605	0.607128	7.047246	0.533764	0.269329	50%	50%

Until now, breast cancer is a type of cancer with the largest number of cases in the world, as well as the highest cause of death. In Indonesia, breast cancer occupies the second rank after cervical cancer. Some breast cancers are associated with a typical genetic mutation. Women with this gene mutation have an 80-90% chance of developing breast cancer. In breast cancer patients, the impact that can arise is the loss of breast due to breast removal surgery. Apart from that, these cancer cells can also spread to other vital organs such as liver, bones, etc. Study by [37] reported that a significant number of cancers (30-65%) can be visualized on prior mammograms on retrospective review. Double reading of mammograms by two radiologists can improve the detection rate of cancer but is expensive and time consuming. The goal of Computer Aided Diagnosis (CAD) is to improve detection rates in a more efficient and cost-effective manner, as human examination of images is often influenced by various factors such as fatigue, carelessness, and others. The detection accuracy is also confined by the limitations of the human visual system. In addition to all these factors, a shortage of qualified radiologists also causes an urgent demand for the development of computer technologies. In this case, the developed CAD algorithm with accuracy of 97% would somehow shed the lights in the field of early breast cancer detection system.

CONCLUSIONS

Breast cancer can be diagnosed with various screening mechanisms, including mammography, however understanding the mammogram images in the phase of diagnosis is not an easy job. Computer Aided Diagnosis (CAD) are seen as tools that can help radiologist for automatic detection of breast cancer. This research presents a method for building a classification system, especially to obtain the different characteristics of mass and micro calcification using association technique based on classification. The outcome of this research has the potential to help radiologist in diagnosing breast cancer by categorizing breast cancer as benign or malignant. From the results, it is clear that the provision of color map in the final segmentation outcome can give more accurate information especially in differentiating between cancer and non-cancer images. By using threshold masks on segmentation edge, and morphology dilate and the segmentation of borderline and variation of coloring, provide optimal results to distinguish between a class of objects cancer tissue and non-cancer. In the evaluation stage, 60 samples were used. The classifier developed able to perform well by successfully classifying the cancer and non-cancer (normal) images with the accuracy of 97%. Apart from that, by applying color map to the final results of segmentation provides a more interesting display of information and gives more direction to the purpose of image processing, which distinguishes between cancerous and non-cancerous tissues.

This study could also be improved, here are suggestions proposed: 1 .Improving the quality image is a process very decisive in image processing mammograms .The improvement of the image of a method of research needed to gain special a method of improving the quality image of mammograms for better results .2 This research can be extended using other classification method to improve the accuracy. In this study, the classification only focuses on normal and cancer. However,

https://doi.org/10.25077/jitce.3.02.96-103.2019

cancer can also be further categorized into benign and malignant background in the division of which there are three categories (fat, the glands of fat, solid) and glands. By giving a direct threshold to the edge segmentation mask, and morphology dilate and borderline segmentation and color variation, it gives optimal results to distinguish between classes of objects between cancerous and noncancerous tissues, and hence can further classify the cancer into stage 1, stage 2, stage 3 and stage 4.

ACKNOWLEDGMENT

This research study is funded by Universiti Pendidikan Sultan Idris, Malaysia, under the Special University Research Grant (Fundamental), 2017-0184-109-01.

REFERENCES

- Jemal, A., Bray, F., Center, M. M., Ferlay, J., Ward, E., & Forman, D. (2011). Global cancer statistics. *CA: a cancer journal for clinicians*, *61*(2), 69-90.
- [2] Skaane, P., Bandos, A. I., Gullien, R., Eben, E. B., Ekseth, U., Haakenaasen, U., & Niklason, L. T. (2013). Comparison of digital mammography alone and digital mammography plus tomosynthesis in a population-based screening program. *Radiology*, 267(1), 47-56.
- [3] Health Quality Ontario. (2016). Ultrasound as an adjunct to mammography for breast cancer screening: a health technology assessment. *Ontario health technology* assessment series, 16(15), 1.
- [4] Harms, S. E. (2001). Integration of breast MRI in clinical trials. Journal of Magnetic Resonance Imaging: An Official Journal of the International Society for Magnetic Resonance in Medicine, 13(6), 830-836.
- [5] Cox, R. F., Hernandez-Santana, A., Ramdass, S., McMahon, G., Harmey, J. H., & Morgan, M. P. (2012). Microcalcifications in breast cancer: novel insights into the molecular mechanism and functional consequence of mammary mineralisation. *British journal of cancer*, 106(3), 525.
- [6] Krupinski, E. A. (2010). Current perspectives in medical image perception. Attention, Perception, & Psychophysics, 72(5), 1205-1217.
- [7] Castellino, R. A. (2005). Computer aided detection (CAD): an overview. *Cancer Imaging*, 5(1), 17.
- [8] Cole, E. B., Zhang, Z., Marques, H. S., Edward Hendrick, R., Yaffe, M. J., & Pisano, E. D. (2014). Impact of computer-aided detection systems on radiologist accuracy with digital mammography. *American Journal of Roentgenology*, 203(4), 909-916.
- [9] Jalalian, A., Mashohor, S., Mahmud, R., Karasfi, B., Saripan, M. I. B., & Ramli, A. R. B. (2017). Foundation and methodologies in computer-aided diagnosis systems for breast cancer detection. *EXCLI journal*, *16*, 113.
- [10] The, J. S., Schilling, K. J., Hoffmeister, J. W., Friedmann, E., McGinnis, R., & Holcomb, R. G. (2009). Detection of breast cancer with full-field digital mammography and computer-aided detection. *American journal of roentgenology*, 192(2), 337-340.
- [11] Mordang, J. J., Gubern-Mérida, A., Bria, A., Tortorella, F., Mann, R. M., Broeders, M. J. M., & Karssemeijer, N. (2018). The importance of early detection of calcifications associated with breast cancer in screening. *Breast cancer research and treatment*, *167*(2), 451-458.
- [12] Razek, N. M. A., Yousef, W. A., & Mustafa, W. A. (2013). Microcalcification detection with and without CAD system (LIBCAD): A comparative study. *The*

Egyptian Journal of Radiology and Nuclear Medicine, 44(2), 397-404.

- [13] Stoeblen, F., Landt, S., Ishaq, R., Stelkens-Gebhardt, R., Rezai, M., Skaane, P., & Kuemmel, S. (2011). Highfrequency breast ultrasound for the detection of microcalcifications and associated masses in BI-RADS 4a patients. *Anticancer research*, 31(8), 2575-2581.
- [14] Biswas, R., Nath, A., & Roy, S. (2016, September). Mammogram Classification Using Gray-Level Cooccurrence Matrix for Diagnosis of Breast Cancer. In *Micro-Electronics and Telecommunication Engineering (ICMETE), 2016 International Conference* on (pp. 161-166). IEEE.
- [15] Vujasinovic, T., Pribic, J., Kanjer, K., Milosevic, N. T., Tomasevic, Z., Milovanovic, Z., & Radulovic, M. (2015). Gray-level co-occurrence matrix texture analysis of breast tumor images in prognosis of distant metastasis risk. *Microscopy and Microanalysis*, 21(3), 646-654.
- [16] Pratiwi, M., Harefa, J., & Nanda, S. (2015). Mammograms classification using gray-level cooccurrence matrix and radial basis function neural network. *Procedia Computer Science*, 59, 83-91.
- [17] Abdelrahman, A., & Hamid, O. (2012). Breast Ultrasound Images Enhancement Using Gray Level Co-Occurrence Matrices Quantizing Technique. *International Journal of Information Science*, 2(5), 60-64.
- [18] Lee, J., Reece, G. P., & Markey, M. K. (2012). Breast curvature of the upper and lower breast mound: 3D analysis of patients who underwent breast reconstruction. In 3rd International Conference on 3D Body Scanning Technologies(pp. 171-179).
- [19] Li, C. M., Segars, W. P., Tourassi, G. D., Boone, J. M., & Dobbins, J. T. (2009). Methodology for generating a 3D computerized breast phantom from empirical data. *Medical physics*, 36(7), 3122-3131.
- [20] Nalawade, Y. V. (2009). Evaluation of breast calcifications. *Indian Journal of Radiology & Imaging*, 19(4).
- [21] Rominger, M. B., Steinmetz, C., Westerman, R., Ramaswamy, A., & Albert, U. S. (2015). Microcalcification-Associated Breast Cancer: Presentation, Successful First Excision, Long-Term Recurrence and Survival Rate. *Breast care*, 10(6), 380-385.
- [22] Naseem, M., Murray, J., Hilton, J. F., Karamchandani, J., Muradali, D., Faragalla, H., ... & Brezden-Masley, C. (2015). Mammographic microcalcifications and breast cancer tumorigenesis: a radiologic-pathologic analysis. *BMC cancer*, 15(1), 307.
- [23] Suckling, J., Parker, J., Dance, D., Astley, S., Hutt, I., Boggis, C., ... & Taylor, P. (2015). Mammographic Image Analysis Society (MIAS) database v1. 21.
- [24] Herwanto, A. M. A., & Arymurthy, A. M. (2013). Association technique based on classification for classifying microcalcification and mass in mammogram. *IJCSI International Journal of Computer Science Issues*, 10(1), 1694-0814.
- [25] Gur, D., Abrams, G. S., Chough, D. M., Ganott, M. A., Hakim, C. M., Perrin, R. L., ... & Bandos, A. I. (2009). Digital breast tomosynthesis: observer performance study. *American Journal of Roentgenology*, 193(2), 586-591.
- [26] Bruno, D. O. T., do Nascimento, M. Z., Ramos, R. P., Batista, V. R., Neves, L. A., & Martins, A. S. (2016). LBP operators on curvelet coefficients as an algorithm to describe texture in breast cancer tissues. *Expert Systems* with Applications, 55, 329-340.
- [27] Bandyopadhyay, S. K. (2010). Pre-processing of Mammogram Images. International Journal of Engineering Science and Technology, 2(11), 6753-6758.
- 100 Suzani Mohamad Samuri

- [28] Bandyopadhyay, S. K. (2010). Detection of abnormal masses in mammogram images. *International Journal of Computer Science and Information Technologies*, 1(5), 438-442.
- [29] Bandyopadhyay, S. K., Maitra, I. K., & Kim, T. H. (2011, April). Identification of abnormal masses in digital mammography images. In *Ubiquitous Computing and Multimedia Applications (UCMA), 2011 International Conference on* (pp. 35-41). IEEE.
- [30] Ponraj, D. N., Jenifer, M. E., Poongodi, P., & Manoharan, J. S. (2011). A survey on the preprocessing techniques of mammogram for the detection of breast cancer. *Journal* of Emerging Trends in Computing and Information Sciences, 2(12), 656-664.
- [31] M. Sezgin & B. Sankur (2004). "Survey over image thresholding techniques and quantitative performance evaluation". Journal of Electronic Imaging. **13** (1): 146– 165. <u>doi:10.1117/1.1631315</u>.
- [32] Liu, Dongju (2009). "Otsu method and K-means". *Ninth International Conference on Hybrid Intelligent Systems IEEE.* 1: 344–349.
- [33] Al-Bayati, M., & El-Zaart, A. (2013). Mammogram images thresholding for breast cancer detection using different thresholding methods. *Advances in Breast Cancer Research*, 2(03), 72.
- [34] Shanmugavadivu, P., & Narayanan, S. L. (2013). Segmentation of microcalcifications in mammogram images using intensity-directed region growing. In *Computer Communication and Informatics (ICCCI)*, 2013 International Conference on (pp. 1-6). IEEE.
- [35] Swetha, T. L. V. N., & Bindu, C. H. (2015). Detection of Breast cancer with Hybrid image segmentation and Otsu's thresholding. In *Computing and Network Communications (CoCoNet), 2015 International Conference on* (pp. 565-570).
- [36] Mohanaiah, P., Sathyanarayana, P., & GuruKumar, L. (2013). Image texture feature extraction using GLCM approach. *International journal of scientific and research publications*, 3(5), 1.
- [37] Elmore, J. G., Armstrong, K., Lehman, C. D., & Fletcher, S.
 W. (2005). Screening for breast cancer. *Jama*, 293(10), 1245-1256.

APPENDICES

Table 1. The results from GLCM

Pictures	Contrast	Variance	Std Deviation	Kurtosis	Mean	Smoothness
1) Input file: \Data Training\can	1.027.975	0.395393	0.628802	9.451.290	0.539653	0.283356
cer001.jpg	1 444 677	0.470000	0.000000	0.450.455	0.500500	0.224020
2) Input file: \Data Training\can cer002.jpg	1.441.665	0.479333	0.692339	9.469.165	0.592580	0.324020
3) Input file: \Data Training\can cer004r.jpg	0.745201	0.368605	0.607128	7.047.246	0.533764	0.269329
4) Input file: .\Data Training\can cer005r.jpg	0.656433	0.908943	0.953385	3.050.584	0.969174	0.476150
5) Input file: \Data Training\can cer007r.jpg	0.533837	0.421264	0.649048	5.056.693	0.494182	0.296401
6) Input file: \Data Training\can cer008r.jpg	0.831437	0.364672	0.603880	13.703.958	0.437214	0.267223
7) Input file: \Data Training\can cer009r.jpg	1.786.484	0.756469	0.869752	4.850.012	0.831375	0.430676
8) Input file: \Data Training\can cer010r.jpg	0.805781	0.254647	0.504626	22.838.733	0.292154	0.202963
9) Input file: .\Data Training\can cer011r.jpg	2.895.576	0.772208	0.878753	8.091.002	0.604129	0.435732
cer011r.jpg 10) Input file: .\Data Training\can cer012r.jpg	1.089.179	0.860437	0.927597	2.971.478	1.005.752	0.462492
file: .\Data Training\can cer013.jpg	1.241.824	0.884123	0.940278	3.545.246	0.862658	0.469249
12) Input file: .\Data Training\can cer014r.jpg	0.480968	0.292931	0.541231	3.243.053	0.522723	0.226563
file: .\Data Training\can cer014.jpg	0.659686	0.384301	0.619920	7.606.833	0.553142	0.277614
14) Input file: .\Data Training\can cer016.jpg	0.887930	0.695458	0.833941	5.918.708	0.600904	0.410189
15) Input file: .\Data Training\can cer017.jpg	0.933452	0.342092	0.584886	9.046.787	0.510722	0.254895
16) Input file: .\Data Training\can cer018.jpg	1.046.170	0.268747	0.518408	13.412.767	0.491343	0.211821
17) Input file: .\Data Training\can cer019.jpg	0.339692	0.196974	0.443817	35.674.353	0.145744	0.164560
18) Input file: .\Data Training\can cer020.jpg	0.979368	0.349894	0.591519	7.787.264	0.545829	0.259201
19) Input file: .\Data Training\can cer021.jpg	0.950996	0.545184	0.738366	6.124.198	0.573179	0.352828
20) Input file: .\Data Training\can cer022.jpg	0.925971	1.023.833	1.011.846	2.608.508	1.119.278	0.505888
21) Input file: .\Data Training\can cer023.jpg	1.284.403	0.571494	0.755972	8.212.665	0.612259	0.363663
22) Input file: .\Data Training\can cer024.jpg	1.134.268	0.373243	0.610936	13.794.881	0.485263	0.271797
23) Input file: .\Data Training\can cer025.jpg	0.687896	0.329313	0.573858	5.439.004	0.527263	0.247732
24) Input file: .\Data Training\can cer026.jpg	1.180.353	0.689164	0.830159	5.632.584	0.677333	0.407991

25) Input file: .\Data Training\can cer027.jpg	0.433786	0.600241	0.774752	7.061.940	0.537373	0.375094
26) Input file: .\Data Training\can cer028.jpg	1.357.183	0.323039	0.568365	10.801.558	0.486268	0.244164
27) Input file: .\Data Training\can cer029.jpg	1.166.930	0.543015	0.736895	6.540.144	0.635783	0.351918
28) Input file: .\Data Training\can cer030.jpg	1.086.810	0.269325	0.518965	11.300.005	0.426429	0.212180
29) Input file: .\Data Training\can cer031.jpg	0.979220	0.792064	0.889980	6.060.835	0.582719	0.441984
30) Input file: .\Data Training\can cer032.jpg	0.959707	0.495989	0.704265	7.207.502	0.597488	0.331546
31) Input file: .\Data Training\nor mal001.jpg	0.149032	0.022416	0.149718	26783677	0.142766	0.021924
32) Input file: .\Data Training\nor mal002.jpg	0.396913	0.051596	0.227149	28594185	0.238457	0.049065
33) Input file: .\Data Training\nor mal003.jpg	0.307292	0.030187	0.173743	6682308	0.190521	0.029302
34) Input file: .\Data Training\nor mal005r.jpg	0.777644	0.201198	0.448551	15631640	0.422361	0.167498
35) Input file: .\Data Training\nor mal007r.jpg	1.014.527	0.258868	0.508790	12.827.915	0.420889	0.205635
36) Input file: .\Data Training\nor mal008r.jpg	1.073.570	0.306933	0.554016	8.096.671	0.623820	0.234850
37) Input file: .\Data Training\nor mal009r.jpg	0.751702	0.156533	0.395643	20.118.500	0.355901	0.135347
38) Input file: .\Data Training\nor mal010r.jpg	0.782944	0.110475	0.332378	28.735.658	0.291524	0.099485
39) Input file: .\Data Training\nor mal011r.jpg	0.235302	0.061721	0.248438	89.195.943	0.143664	0.058133
40) Input file: .\Data Training\nor mal012r.jpg	0.328074	0.046063	0.214623	98.636.136	0.169926	0.044035
41) Input file: .\Data Training\nor mal013r.jpg	0.089443	0.016786	0.129561	2.470.104	0.160746	0.016509
42) Input file: .\Data Training\nor mal014r.jpg	0.188233	0.020606	0.143547	3.427.664	0.153428	0.020190
43) Input file: .\Data Training\nor mal015r.jpg	0.084951	0.014619	0.120908	1.526.303	0.139433	0.014408
44) Input file: .\Data Training\nor mal016r.jpg	0.318124	0.051689	0.227352	10.496.390	0.217974	0.049148
45) Input file: .\Data Training\nor mal017r.jpg	0.788998	0.108960	0.330091	26.074.141	0.303300	0.098254
46) Input file: .\Data Training\nor mal018r.jpg	5.408.722	0.157456	0.396807	22.624.975	0.369341	0.136036
47) Input file: .\Data Training\nor mal019r.jpg	0.681340	0.071983	0.268297	10.464.641	0.262203	0.067149
48) Input file: .\Data Training\nor mal020r.jpg	0.620242	0.073724	0.271522	6.439.709	0.255898	0.068662
49) Input file: .\Data Training\nor mal021.jpg	0.688708	0.146310	0.382505	15.293.631	0.323929	0.127635
50) Input file: .\Data	0.257305	0.025060	0.158304	21.863.137	0.183297	0.024448

Training\nor mal022.jpg						
51) Input file: .\Data Training\nor mal023.jpg	0.096304	0.014161	0.118998	2.025.034	0.097940	0.013963
52) Input file: .\Data Training\nor mal024.jpg	0.077927	0.015871	0.125979	1.285.351	0.147853	0.015623
53) Input file: .\Data Training\nor mal025.jpg	0.515347	0.324569	0.569710	21.491.535	0.307629	0.245038
54) Input file: .\Data Training\nor mal026.jpg	0.255861	0.015645	0.125080	1.579.303	0.110151	0.015404
55) Input file: .\Data Training\nor mal027.jpg	0.323657	0.035670	0.188865	43.388.443	0.167092	0.034442
56) Input file: .\Data Training\nor mal028.jpg	0.148797	0.018848	0.137288	1.819.557	0.181640	0.018499
57) Input file: .\Data Training\nor mal029.jpg	0.121953	0.020460	0.143038	10.173.960	0.159180	0.020050
58) Input file: .\Data Training\nor mal030.jpg	3.370.836	0.057243	0.239255	24.555.437	0.260783	0.054144
59) Input file: .\Data Training\nor mal031.jpg	0.620382	0.054293	0.233008	19.159.720	0.263466	0.051497
60) Input file: .\Data Training\nor mal032.jpg	0.191360	0.025589	0.159964	37.869.866	0.181133	0.024950

Table 2. The evaluation results

Picture	Contrast	Varia	Std Dev	Kurto	Mea	Smooth	Corre	Incorre
		nce		sis	n	ness	ct	ct
 Input file: .\Data Training\ cancer00 1.jpg 	1.027.975	0.395 393	0.6288 02	9.451 .290	0.539 653	0.2833 56	50,00 %	50,00%
2) Input file: .\Data Training\ cancer00 2.jpg	1.441.665	0.479 333	0.6923 39	9.469 .165	0.592 580	0.3240 20	50,00 %	50,00%
3) Input file: .\Data Training\ cancer00 4r.jpg	0.745201	0.368 605	0.6071 28	7.047 .246	0.533 764	0.2693 29	50,00 %	50,00%
4) Input file: .\Data Training\ cancer00 5r.jpg	0.656433	0.908 943	0.9533 85	3.050 .584	0.969 174	0.4761 50	50,00 %	50,00%
5) Input file: .\Data Training\ cancer00 7r.jpg	0.533837	0.421 264	0.6490 48	5.056 .693	0.494 182	0.2964 01	50,00 %	50,00%
6) Input file: .\Data Training\ cancer00 8r.jpg	0.831437	0.364 672	0.6038 80	13.70 3.958	0.437 214	0.2672 23	50,00 %	50,00%
7) Input file: .\Data Training\ cancer00 9r.jpg	1.786.484	0.756 469	0.8697 52	4.850 .012	0.831 375	0.4306 76	50,00 %	50,00%
8) Input file: .\Data Training\ cancer01 0r.jpg	0.805781	0.254 647	0.5046 26	22.83 8.733	0.292 154	0.2029 63	50,00 %	50,00%
9) Input file: .\Data Training\ cancer01 1r.jpg	2.895.576	0.772 208	0.8787 53	8.091 .002	0.604 129	0.4357 32	50,00 %	50,00%

10) Input file: .\Data Training\ cancer01 2r ing	1.089.179	0.860 437	0.9275 97	2.971 .478	1.005 .752	0.4624 92	50,00 %	50,00
2r.jpg	4.944.000			3.575				
11) Input file: .\Data Training\ cancer01 3.jpg	1.241.824	0.884 123	0.9402 78	3.545 .246	0.862 658	0.4692 49	50,00 %	50,00
12) Input file: .\Data Training\ cancer01	0.480968	0.292 931	0.5412 31	3.243 .053	0.522 723	0.2265 63	50,00 %	50,00
4r.jpg								
13) Input file: .\Data Training\ cancer01 5.jpg	0.659686	0.384 301	0.6199 20	7.606	0.553 142	0.2776 14	50,00 %	50,00
14) Input file: .\Data Training\ cancer01 6.jpg	0.887930	0.695 458	0.8339 41	5.918 .708	0.600 904	0.4101 89	50,00 %	50,00
15) Input file: .\Data Training\ cancer01	0.933452	0.342 092	0.5848 86	9.046 .787	0.510 722	0.2548 95	50,00 %	50,00
7.jpg 16) Input file: .\Data Training\ cancer01 8.jpg	1.046.170	0.268 747	0.5184 08	13.41 2.767	0.491 343	0.2118 21	50,00 %	50,00
17) Input file: .\Data Training\ cancer01 9.jpg	0.339692	0.196 974	0.4438 17	35.67 4.353	0.145 744	0.1645 60	50,00 %	50,00
18) Input file: .\Data Training\ cancer02 0.jpg	0.979368	0.349 894	0.5915 19	7.787 .264	0.545 829	0.2592 01	50,00 %	50,00
19) Input file: .\Data Training\ cancer02 1.jpg	0.950996	0.545 184	0.7383 66	6.124 .198	0.573 179	0.3528 28	50,00 %	50,00
20) Input file: .\Data Training\ cancer02 2.jpg	0.925971	1.023 .833	1.011.8 46	2.608 .508	1.119 .278	0.5058 88	50,00 %	50,00
21) Input file: .\Data Training\ cancer02 3.jpg	1.284.403	0.571 494	0.7559 72	8.212 .665	0.612 259	0.3636 63	50,00 %	50,00
22) Input file: .\Data Training\ cancer02 4.jpg	1.134.268	0.373 243	0.6109 36	13.79 4.881	0.485 263	0.2717 97	50,00 %	50,00
23) Input file: .\Data Training\ cancer02 5.jpg	0.687896	0.329 313	0.5738 58	5.439 .004	0.527 263	0.2477 32	50,00 %	50,00
24) Input file: .\Data Training\ cancer02 6.jpg	1.180.353	0.689 164	0.8301 59	5.632 .584	0.677 333	0.4079 91	50,00 %	50,00
25) Input file: .\Data Training\ cancer02 7.jpg	0.433786	0.600 241	0.7747 52	7.061 .940	0.537 373	0.3750 94	50,00 %	50,00
26) Input file: .\Data Training\ cancer02 8.jpg	1.357.183	0.323 039	0.5683 65	10.80 1.558	0.486 268	0.2441 64	50,00 %	50,00

27) Input file:	1.166.930	0.543	0.7368	6.540 .144	0.635	0.3519	50,00 %	50,00%
Ille: .\Data Training\ cancer02 9.jpg		0.543	95	.144	783	18	26	
28) Input	1.086.810			11.30			50,00	50,00%
file: .\Data Training\ cancer03 0.jpg		0.269 325	0.5189 65	0.005	0.426 429	0.2121 80	%	
29) Input file: .\Data Training\ cancer03 1.jpg	0.979220	0.792 064	0.8899 80	6.060 .835	0.582 719	0.4419 84	50,00 %	50,00%
30) Input file: .\Data Training\ cancer03 2.jpg	0.959707	0.495 989	0.7042 65	7.207 .502	0.597 488	0.3315 46	50,00 %	50,00%
31) Input file: .\Data Training\ normal00 1.jpg	0.149032	0.022 416	0.1497 18	2678 3677	0.142 766	0.0219 24	100,0 0%	0,00%
32) Input file: .\Data Training\ normal00	0.396913	0.051 596	0.2271 49	2859 4185	0.238 457	0.0490 65	100,0 0%	0,00%
2.jpg 33) Input file: .\Data Training\ normal00 3.jpg	0.307292	0.030 187	0.1737 43	6682 308	0.190 521	0.0293 02	100,0 0%	0,00%
34) Input file: .\Data Training\ normal00 5r.jpg	0.777644	0.201 198	0.4485 51	1563 1640	0.422 361	0.1674 98	100,0 0%	0,00%
35) Input file: .\Data Training\ normal00 7r.jpg	1.014.527	0.258 868	0.5087 90	12.82 7.915	0.420 889	0.2056 35	100,0 0%	0,00%
36) Input file: .\Data Training\ normal00	1.073.570	0.306 933	0.5540 16	8.096	0.623 820	0.2348 50	0,00 %	100,00 %
8r.jpg 37) Input file: .\Data Training\ normal00 9r.jpg	0.751702	0.156 533	0.3956 43	20.11 8.500	0.355 901	0.1353 47	100,0 0%	0,00%
38) Input file: .\Data Training\ normal01 0r.jpg	0.782944	0.110 475	0.3323 78	28.73 5.658	0.291 524	0.0994 85	100,0 0%	0,00%
39) Input file: .\Data Training\ normal01 1r.jpg	0.235302	0.061 721	0.2484 38	89.19 5.943	0.143 664	0.0581 33	100,0 0%	0,00%
40) Input file: .\Data Training\ normal01 2r.jpg	0.328074	0.046 063	0.2146 23	98.63 6.136	0.169 926	0.0440 35	100,0 0%	0,00%
41) Input file: .\Data Training\ normal01 3r.jpg	0.089443	0.016 786	0.1295 61	2.470 .104	0.160 746	0.0165 09	100,0 0%	0,00%
42) Input file: .\Data Training\ normal01 4r.jpg	0.188233	0.020 606	0.1435 47	3.427 .664	0.153 428	0.0201 90	100,0 0%	0,00%
43) Input file: .\Data Training\ normal01 5r.jpg	0.084951	0.014 619	0.1209 08	1.526 .303	0.139 433	0.0144 08	100,0 0%	0,00%

44) Input file: .\Data Training\ normal01	0.318124	0.051 689	0.2273 52	10.49 6.390	0.217 974	0.0491 48	100,0 0%	0,00%
6r.jpg 45) Input file:	0.788998	0.108	0.3300	26.07 4.141	0.303	0.0982	100,0 0%	0,00%
.\Data Training\ normal01 7r.jpg		960	91		300	54		
46) Input file: .\Data Training\ normal01 8r.jpg	5.408.722	0.157 456	0.3968 07	22.62 4.975	0.369 341	0.1360 36	0,00 %	100,00 %
47) Input file: .\Data Training\ normal01 9r.jpg	0.681340	0.071 983	0.2682 97	10.46 4.641	0.262 203	0.0671 49	100,0 0%	0,00%
48) Input file: .\Data Training\ normal02 0r.jpg	0.620242	0.073 724	0.2715 22	6.439 .709	0.255 898	0.0686 62	100,0 0%	0,00%
49) Input file: .\Data Training\ normal02 1.jpg	0.688708	0.146 310	0.3825 05	15.29 3.631	0.323 929	0.1276 35	100,0 0%	0,00%
50) Input file: .\Data Training\ normal02 2.jpg	0.257305	0.025 060	0.1583 04	21.86 3.137	0.183 297	0.0244 48	100,0 0%	0,00%
51) Input file: .\Data Training\ normal02 3.jpg	0.096304	0.014 161	0.1189 98	2.025 .034	0.097 940	0.0139 63	100,0 0%	0,00%
52) Input file: .\Data Training\ normal02	0.077927	0.015 871	0.1259 79	1.285 .351	0.147 853	0.0156 23	100,0 0%	0,00%
4.jpg 53) Input file: .\Data Training\ normal02	0.515347	0.324 569	0.5697 10	21.49 1.535	0.307 629	0.2450 38	100,0 0%	0,00%
5.jpg 54) Input file: .\Data Training\ normal02 6.jpg	0.255861	0.015 645	0.1250 80	1.579 .303	0.110 151	0.0154 04	100,0 0%	0,00%
55) Input file: .\Data Training\ normal02 7.jpg	0.323657	0.035 670	0.1888 65	43.38 8.443	0.167 092	0.0344 42	100,0 0%	0,00%
56) Input file: .\Data Training\ normal02 8.jpg	0.148797	0.018 848	0.1372 88	1.819 .557	0.181 640	0.0184 99	100,0 0%	0,00%
57) Input file: .\Data Training\ normal02 9.jpg	0.121953	0.020 460	0.1430 38	10.17 3.960	0.159 180	0.0200 50	100,0 0%	0,00%
5.jpg 58) Input file: .\Data Training\ normal03 0.jpg	3.370.836	0.057 243	0.2392 55	24.55 5.437	0.260 783	0.0541 44	100,0 0%	0,00%
59) Input file: .\Data Training\ normal03 1.jpg	0.620382	0.054 293	0.2330 08	19.15 9.720	0.263 466	0.0514 97	100,0 0%	0,00%
60) Input file: .\Data Training\ normal03	0.191360	0.025 589	0.1599 64	37.86 9.866	0.181 133	0.0249 50	100,0 0%	0,00%

https://doi.org/10.25077/jitce.3.02.96-103.2019